

# Quantitative analysis of protein–ligand interactions by NMR



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## ABSTRACT

Protein–ligand interactions have been commonly studied through static structures of the protein–ligand complex. Recently, however, there has been increasing interest in investigating the dynamics of protein–ligand interactions both for fundamental understanding of the underlying mechanisms and for drug development. NMR is a versatile and powerful tool, especially because it provides site-specific quantitative information. NMR has widely been used to determine the dissociation constant ( $K_D$ ), in particular, for relatively weak interactions. The simplest NMR method is a chemical-shift titration experiment, in which the chemical-shift changes of a protein in response to ligand titration are measured. There are other quantitative NMR methods, but they mostly apply only to interactions in the fast-exchange regime. These methods derive the dissociation constant from population-averaged NMR quantities of the free and bound states of a protein or ligand. In contrast, the recent advent of new relaxation-based experiments, including  $R_2$  relaxation dispersion and ZZ-exchange, has enabled us to obtain kinetic information on protein–ligand interactions in the intermediate- and slow-exchange regimes. Based on  $R_2$  dispersion or ZZ-exchange, methods that can determine the association rate,  $k_{on}$ , dissociation rate,  $k_{off}$ , and  $K_D$  have been developed. In these approaches,  $R_2$  dispersion or ZZ-exchange curves are measured for multiple samples with different protein and/or ligand concentration ratios, and the relaxation data are fitted to theoretical kinetic models. It is critical to choose an appropriate kinetic model, such as the two- or three-state exchange model, to derive the correct kinetic information. The  $R_2$  dispersion and ZZ-exchange methods are suitable for the analysis of protein–ligand interactions with a micromolar or sub-micromolar dissociation constant but not for very weak interactions, which are typical in very fast exchange. This contrasts with the NMR methods that are used to analyze population-averaged NMR quantities. Essentially, to apply NMR successfully, both the type of experiment and equation to fit the data must be carefully and specifically chosen for the protein–ligand interaction under analysis. In this review, we first explain the exchange regimes and kinetic models of protein–ligand interactions, and then describe the NMR methods that quantitatively analyze these specific interactions.

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## 1. Introduction

Proteins interact with various ligand molecules, such as peptides, proteins, nucleic acids, and small organic compounds, and these interactions play central roles in biological systems [1,2]. Details of such interactions (hereafter termed protein–ligand interactions) have been studied by solving structures of the protein–ligand complex using X-ray crystallography and NMR spectroscopy. The complex structures, which are determined as static pictures, provide information on site-specific interactions between a protein and a ligand molecule. If the structure of the free state of the protein is determined as well as the complex structure, the conformational changes upon ligand binding can also be understood. Such structural information is often utilized for drug development [3].

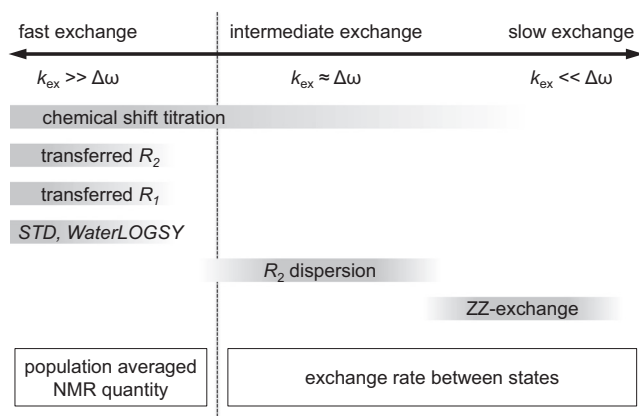
Recently, in addition to attempts to understand protein–ligand interactions from static pictures [4], there is an increasing interest in investigating the dynamic processes of protein–ligand interactions so as to improve our fundamental understanding of their mechanisms [5,6]. Protein–ligand interactions can be studied by several biophysical techniques [7], including ultraviolet/visible absorption spectroscopy [8], analytical ultracentrifugation [9], circular dichroism [10], fluorescence spectroscopy [11], differential scanning fluorimetry [12], surface plasmon resonance [13], isothermal titration calorimetry (ITC) [14], quartz crystal microbalance [15], mass spectrometry [16], small-angle X-ray scattering [17], atomic force microscopy [18], and NMR [19]. These provide information that is difficult to derive from a static structure alone—for example, kinetic parameters, thermodynamic parameters, dissociation constants, and conformational changes upon ligand binding. Among them, NMR is the most versatile and powerful tool with which to study the dynamics of protein–ligand interactions, especially because it provides site-specific quantitative information [19].

With regard to quantitative NMR analysis of protein–ligand interactions, NMR has most widely been used to determine the dissociation constant,  $K_D$  [20,21], in particular, for relatively weak interactions ( $K_D > 10 \mu\text{M}$ ) that would be difficult to investigate by other biophysical methods [22]. Dissociation constants are most simply determined from the chemical-shift changes of a protein in response to ligand titration [23]; this method is designated chemical-shift titration. Concomitantly, the binding site on the surface of the protein can also be roughly identified from chemical shift data because the chemical shifts of the protein are altered both by direct contact with the ligand and by its own conformational changes that occur upon ligand binding. This method is one of the simplest and earliest to be applied in this field, but it can be easily used to examine whether a ligand binds to its target protein and vice versa.

There are other quantitative NMR methods (Fig. 1), but most of them can be applied only to interactions in the fast-exchange regime (see Section 2.1). They are mainly used to derive dissociation constants, using population-averaged NMR observable quantities of the free and bound states of a protein or ligand. This type of NMR method includes the chemical-shift titration experiment, in which population-averaged chemical shifts of the free and bound states are observed during a ligand titration. In addition to chemical shift, the population-averaged longitudinal relaxation rate  $R_1$  and transverse relaxation rate  $R_2$  can also be used to determine dissociation constants.

By contrast, some NMR relaxation experiments, such as relaxation dispersion [24–26] and ZZ-exchange spectroscopy [27], can provide the exchange rates of a protein and are capable of analyzing interactions in the intermediate- and slow-exchange regimes. These methods have been applied to many protein–ligand interactions in order to understand their mode of action from the viewpoint of protein dynamics [28–38]. In particular there are recently developed methods that can determine the association rate,  $k_{\text{on}}$ , dissociation rate,  $k_{\text{off}}$ , and  $K_D$  [30,31,37], using  $R_2$  relaxation dispersion or ZZ-exchange curves measured for multiple samples with different protein/ligand concentration ratios, similarly to the ligand titration experiment. The relaxation or ZZ-exchange curves obtained are then fitted to theoretical kinetic models [39]. These methods are suitable for the analysis of protein–ligand interactions with a micromolar or sub-micromolar dissociation constant, but not for very weak interactions, which are typically in very fast exchange. This contrasts with the above-mentioned quantitative NMR methods that are used to analyze population-averaged NMR quantities (Fig. 1). Therefore, it is essential to choose carefully an appropriate method for the protein–ligand interaction under analysis.

In this review, we first explain the exchange regimes and kinetic models of protein–ligand interactions in equilibrium. We then describe the NMR methods that can analyze protein–ligand interactions quantitatively, with a particular focus on relatively new methods that utilize NMR relaxation measurements and on features of the interactions that define which of the NMR methods is applicable.



**Fig. 1.** NMR methods used for quantitative analysis of protein–ligand interactions. NMR methods described in the main text are shown along with the chemical shift timescales.  $k_{\text{ex}}$  denotes the exchange rate, which is defined as the sum of the forward and backward rates in units of  $\text{s}^{-1}$ :  $k_{\text{ex}} = [B]k_{\text{on}} + k_{\text{off}}$ .  $\Delta\omega$  denotes the chemical shift difference between the free and bound states in units of  $\text{rad s}^{-1}$ .

## 2. Theoretical aspects of protein–ligand interactions

To analyze protein–ligand interactions quantitatively by NMR, an appropriate method should be carefully chosen in accordance with the chemical exchange regime of the interaction on the chemical shift timescale. Furthermore, in the case of NMR methods that deal with the kinetic rates of the interaction, an appropriate interaction model, such as a two- or three-state exchange model, must be chosen to analyze the data because—except for very slow interactions on a timescale of seconds or slower—protein–ligand interactions are difficult to analyze directly in real time by NMR [40,41]. Therefore, the collected NMR data are fitted to a theoretical equation derived for a specific interaction model after the NMR measurements have been completed. Multiple models are usually tested, and the most physiologically and statistically reasonable model is chosen by assessing both the fitting quality and the parameters obtained. In this section, we explain the chemical exchange regimes with a specific focus on protein–ligand interactions and their kinetic models.

### 2.1. Exchange regime

Protein–ligand interactions are schematically represented as equilibrium equations; non-equilibrium interactions such as enzyme reactions are beyond the scope of this review. Most NMR studies of protein–ligand interactions are based on a two-state exchange model:



where A, B, and A:B denote the protein, ligand, and the protein–ligand complex, respectively. In typical protein NMR experiments,

A is an isotope  $^{15}\text{N}$  and/or  $^{13}\text{C}$ -labeled protein and B is unlabeled ligand. [B] denotes the concentration of free B, which can be calculated from the total concentrations of A ( $[A]_0$ ) and B ( $[B]_0$ ), and the dissociation constant  $K_D$ :

$$[B] = \frac{1}{2} \left\{ -K_D - [A]_0 + [B]_0 + \sqrt{(K_D + [A]_0 - [B]_0)^2 + 4[B]_0 K_D} \right\} \quad (2)$$

$$K_D = \frac{k_{\text{off}}}{k_{\text{on}}} = \frac{[A][B]}{[A : B]} \quad (3)$$

The parameters that characterize the chemical exchange regime of a protein–ligand interaction are the exchange rate,  $k_{\text{ex}}$  (in units of  $\text{s}^{-1}$ ), and the chemical-shift difference between the free and bound states,  $\Delta\omega$  (in units of  $\text{rad s}^{-1}$ ) [42].  $\Delta\omega$  is calculated from the chemical-shift difference in units of ppm ( $\Delta\delta$ ) as:

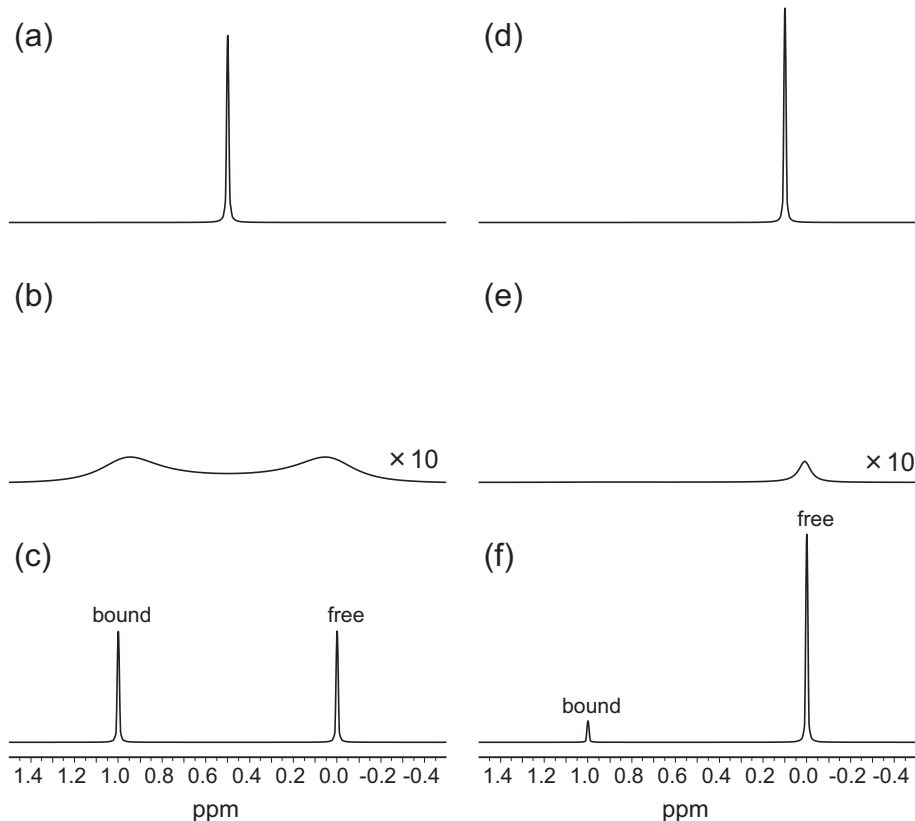
$$\Delta\omega = 2\pi\Delta\delta B_0 \quad (4)$$

where  $B_0$  denotes the magnetic field in units of Hz. For a strong interaction ( $K_D < 0.1 \mu\text{M}$ ), the free and bound resonances of a protein are directly observed by using samples with and without ligand, respectively. For a weak interaction ( $K_D > 10 \mu\text{M}$ ), by contrast, the observable chemical shift difference  $\Delta\delta_{\text{obs}}$  at a 1:1 concentration ratio is usually smaller than the exact chemical shift difference,  $\Delta\delta$ , because the protein is not fully saturated by the ligand. Thus, an excess of ligand should be mixed with the protein to obtain the exact  $\Delta\delta$  value. Alternatively,  $\Delta\delta$  can be estimated by a chemical shift titration experiment (see Section 3.3).

In the case of the two-state exchange model (Eq. (1)),  $k_{\text{ex}}$  is defined as sum of the forward and backward rates:

$$k_{\text{ex}} = [B]k_{\text{on}} + k_{\text{off}} \quad (5)$$

Fig. 2 shows simulated NMR spectra of protein–ligand interactions at  $k_{\text{ex}}$  rates of  $10^6$ ,  $10^3$ , and  $1 \text{ s}^{-1}$ . The population of the bound state is 0.5 in Fig. 2a–c, and 0.1 in Fig. 2d–f. Free and bound



**Fig. 2.** Chemical exchange in a two-state exchange model. (a, d) Fast exchange, (b, e) intermediate exchange, and (c, f) slow exchange. The spectra were simulated by using  $\Delta\omega = 3141 \text{ rad s}^{-1}$  (1 ppm at a  $B_0$  frequency of 500 MHz), and  $k_{\text{ex}} = 10^6 \text{ s}^{-1}$  (a, d),  $10^3 \text{ s}^{-1}$  (b, e), and  $1 \text{ s}^{-1}$  (c, f). The populations of the bound states were 0.5 (a–c) and 0.1 (d–f), and the intrinsic transverse relaxation rates of the free and bound states were both set to  $10 \text{ s}^{-1}$ . The vertical direction in (b) and (e) is expanded 10-fold.

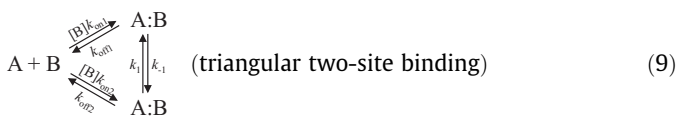
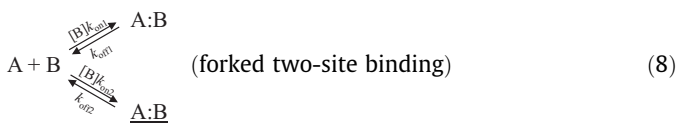
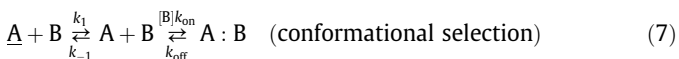
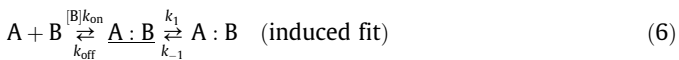
resonances appear at 0 and 1 ppm, respectively; therefore,  $\Delta\omega$  is  $3141 \text{ rad s}^{-1}$  at  $B_0 = 500 \text{ MHz}$ . The intrinsic relaxation rates of the free and bound resonances are both set to  $10 \text{ s}^{-1}$ .

If  $k_{\text{ex}}$  is much larger than  $\Delta\omega$  ( $k_{\text{ex}} \gg \Delta\omega$ ), the interaction is in the fast-exchange regime, and an NMR signal appears at the population-averaged chemical shift of the free and bound states (Fig. 2a and d). If  $k_{\text{ex}}$  is comparable in magnitude to  $\Delta\omega$  ( $k_{\text{ex}} \approx \Delta\omega$ ), the interaction is in the intermediate exchange regime, and the NMR signal becomes broad owing to the contribution of transverse relaxation due to chemical exchange, termed  $R_{\text{ex}}$  (Fig. 2b and e). When the population is highly skewed, as in the case where the bound population is 0.1 (Fig. 2e), the resonance of the minor state is unobservable. This often happens in titration experiments. If  $k_{\text{ex}}$  is much smaller than  $\Delta\omega$  ( $k_{\text{ex}} \ll \Delta\omega$ ), the interaction is in the slow-exchange regime, and a pair of NMR signals corresponding to the free and bound states appears at different chemical shifts (Fig. 2c and f). Provided that the relaxation rates of the free and bound resonances are identical, the signal intensities are proportional to the fraction of the corresponding states.

These classifications of the exchange regime are the same as those of chemical (conformational) exchange in a molecule, but it should be emphasized that the exchange regime of a protein–ligand interaction can change according to the concentrations of A and B. Although  $\Delta\omega$  is invariant at any concentration of A and B,  $k_{\text{ex}}$  is dependent on concentration (Eqs. (2) and (5)). This property of chemical exchange must be taken into account when a protein–ligand interaction is quantitatively analyzed by NMR, especially by the chemical-shift titration experiment. In some cases, the exchange regime of the interactions can change from slow to intermediate to fast exchange during ligand titration (see Section 3.3).

## 2.2. Kinetic model

In the previous section, we explained the kinetics established for the two-state exchange model (Eq. (1)). In addition to the two-state exchange model, some interaction studies using NMR, especially relaxation dispersion spectroscopy, use three-state exchange models, for which four different kinetic binding models can be constructed: induced fit [43], conformational selection (pre-equilibrium) [44], forked two-site binding, and triangular two-site binding models.



where underscored letters represent the states whose conformations are different from that of the other free or bound state in the same model. The induced fit model has an on-pathway binding intermediate state in-between the free and bound states (Eq. (6)). In this model, the protein adjusts its conformation to fit the shape of its binding site after the ligand binds. The conformational selection model, originally called the pre-equilibrium model, has two free states that interconvert with each other (Eq. (7)). In this model,

the protein adopts a bound-like conformation before the ligand binds, and this free state then proceeds to the bound state. The forked two-site binding model has an off-pathway bound state in addition to the correct bound state (Eq. (8)), but the two bound states do not interconvert with each other. In contrast to the forked two-site binding model, the triangular two-site binding model has two bound states that do interconvert (Eq. (9)). In addition to these four models, one more three-state exchange model can theoretically be constructed; this model is the same as the conformational selection model except that both free states proceed to the same bound state. This model, however, seems physiologically unreasonable because the same bound conformation is formed from two different free conformations with no intermediate in either pathway.

Eq. (2) is valid for all the three-state exchange models, but the definitions of  $K_D$  differ from Eq. (3):

$$K_D = \frac{k_{\text{off}}}{k_{\text{on}}} \times \frac{k_{-1}}{k_1 + k_{-1}} \quad (\text{induced fit}) \quad (10)$$

$$K_D = \frac{k_{\text{off}}}{k_{\text{on}}} \times \frac{k_1 + k_{-1}}{k_1} \quad (\text{conformational selection}) \quad (11)$$

$$K_D = \frac{k_{\text{off}1}k_{\text{off}2}}{k_{\text{on}1}k_{\text{off}2} + k_{\text{on}2}k_{\text{off}1}} \quad (\text{forked two-site binding}) \quad (12)$$

$$K_D = \frac{k_{\text{off}1}k_{\text{off}2} + k_{\text{off}1}k_{-1} + k_{\text{off}2}k_1}{k_{\text{on}1}(k_{\text{off}2} + k_1 + k_{-1}) + k_{\text{on}2}(k_{\text{off}1} + k_1 + k_{-1})} \quad (\text{triangular two-site binding}) \quad (13)$$

These equations including Eq. (2) are derived by using the principle of microscopic reversibility. For example, in the case of the induced fit model, Eqs. (2) and (10) are derived by solving the following simultaneous equations:

$$\begin{cases} [A][B]k_{\text{on}} = [\underline{A:B}]k_{\text{off}} \\ [\underline{A:B}]k_1 = [A:B]k_{-1} \\ [A] + [\underline{A:B}] + [A:B] = [A]_0 \\ [B] + [\underline{A:B}] + [A:B] = [B]_0 \end{cases} \quad (14)$$

## 3. Protein–ligand interaction in the fast-exchange regime

To quantitatively analyze protein–ligand interactions in the fast-exchange regime, saturation transfer difference (STD) [45,46] and water–ligand observed via gradient spectroscopy (WaterLOGSY) [47,48] have been widely used, in particular for drug screening. Here we only briefly explain these two NMR methods, before describing in more detail other methods based on the fact that some NMR quantities, such as the longitudinal relaxation rate  $R_1$ , transverse relaxation rate  $R_2$ , and chemical shift  $\delta$ , are observed as population-averaged values of the free and bound states during fast exchange. The NMR methods that analyze population-averaged  $R_1$ ,  $R_2$ , and  $\delta$  are called transferred  $R_1$  [49], transferred  $R_2$  [50], and chemical shift titration, respectively. They have been used to determine  $K_D$  but not kinetic rates, except for some recent analyses of chemical shift titration data.

### 3.1. STD and WaterLOGSY

Saturation transfer difference (STD) and water–ligand observed via gradient spectroscopy (WaterLOGSY) are typically used for screening ligands that bind to a protein with  $K_D$  in the range of  $10^{-3}$  to  $10^{-8} \text{ M}$  [51]. The samples analyzed by these NMR methods contain a ligand or a mixture of ligands in the presence of a small amount of a protein. The  $^1\text{H}$  resonances of the bound ligand are perturbed, and the perturbed magnetization is transferred to the



$^1\text{H}$  resonances of the free ligand via fast chemical exchange. Therefore, the NMR signals of the interaction sites on the ligand can be detected. The pathway of the magnetization transfer is different between STD and WaterLOGSY. In the case of WaterLOGSY, the  $^1\text{H}$  resonance of bulk water are excited and the magnetization is transferred from transiently bound water to the bound ligand. Magnetization transfer may also occur via indirect spin diffusion through exchangeable and nonexchangeable  $^1\text{H}$  of the protein. In the case of STD, a selected  $^1\text{H}$  spectral region of the protein is saturated, which causes saturation of additional  $^1\text{H}$  resonances of the protein via spin diffusion and magnetization transfer from the protein to the ligand via intermolecular NOEs.

Because the NMR signals of the ligand are analyzed, these methods are called ligand-based NMR techniques. In addition, because the NMR signals of the protein are not observed, the protein can be very large (>50 kDa) and does not have to be isotope-labeled. Furthermore, the amount of protein is usually not very high (micromolar range) [52]. STD and WaterLOGSY can probe weak interactions that are difficult to detect by other biophysical experiments, and the analytical samples can contain a mixture of ligands [47]; therefore, they are widely used for drug screening. The identified ligands are then optimized by using combinatorial chemistry and structure-based drug design, among other techniques [53]. Recently, Antanasijevic et al. [54] compared the sensitivities of STD and WaterLOGSY using three experimental systems: ketoprofen–bovine serum albumin, tert-butyl hydroquinone–hemagglutinin, and chloramphenicol–ribosome. The authors found that WaterLOGSY was more sensitive than STD in all three systems [54]. They attribute the higher sensitivity of WaterLOGSY to be due to simultaneous saturation of multiple sources of cross correlation, including direct NOEs of water and exchangeable groups and indirect NOEs of  $^1\text{H}$ –C groups.

### 3.2. Transferred $R_1$ and transferred $R_2$

LaPlante et al. [49] developed the transferred  $R_1$  method, in which relative changes in the  $R_1$  relaxation rate of a ligand (an isotope-labeled small protein) in the free state and in the presence of a small amount of the target protein are measured. In the case of fast exchange, the longitudinal relaxation rate  $R_{1av}$  is measured as a population-averaged value of the free and bound states of the ligand:

$$R_{1av} = p_F R_{1F} + p_B R_{1B} \quad (15)$$

where  $p_F$  and  $p_B$  denote the fraction of the ligand in the free and bound states, respectively, and  $R_{1F}$  and  $R_{1B}$  are the longitudinal relaxation rates of the ligand in the free and the bound states, respectively. Note that the transferred  $R_1$  method can be applied only if the ligand has a large difference between its  $R_{1F}$  and  $R_{1B}$  values. If  $R_{1F}$  and  $R_{1B}$  are comparable,  $R_{1av}$  does not change no matter how much protein is added to the ligand solution. Also, because the longitudinal rate  $R_1$  decreases with increasing molecular weight, the protein that is titrated into the ligand must be much larger than the ligand in order to obtain a sufficient difference between the  $R_{1F}$  and  $R_{1av}$  rates. How much difference is required depends on the quality of the NMR data. Thus, it is a good strategy to simulate transferred  $R_1$  profiles using  $R_1$  values of the protein and ligand that are estimated from their molecular weights and including a certain experimental error before conducting the NMR measurements. If  $R_{1av}$  is measured for multiple samples with different protein/ligand concentration ratios and  $R_{1av}$  changes with the concentration ratio, then  $K_D$  can be derived from the following equation:

$$K_D = \frac{p_F}{p_B} ([B]_0 - p_B [A]_0) \quad (16)$$

which in turn is derived from the definition of  $K_D = [A][B]/[A:B]$  for the two-state exchange model (Eq. (1)). LaPlante et al. [49] applied the transferred  $R_1$  method to BILN127SE, an inhibitor of the non-structural 3 protease domain of the hepatitis C virus, and used variations in the  $R_1$  values for different residues to characterize the local dynamics of the inhibitor rather than determining the  $K_D$  value.

The transferred  $R_2$  method is similar to the transferred  $R_1$  method ( $R_1$  in Eq. (15) is simply replaced by  $R_2$ ), but is comparatively more sensitive to protein–ligand interactions because the difference in the relaxation rate between the free and bound states is usually larger for  $R_2$  than for  $R_1$  [50]. In contrast to  $R_1$ , the transverse relaxation rate  $R_2$  increases with increasing molecular weight. Note that the transferred  $R_2$  method can be applied only if the interaction is sufficiently fast to prevent any contribution to the measured  $R_2$  rate from chemical exchange between the free and bound states, and if the exchange rate is faster than the  $R_2$  rate of the bound state. Using the transferred  $R_2$  method, Su et al. [50] determined  $K_D$  for the interaction between the  $\tau$  subunit of the *Escherichia coli* DNA polymerase III complex (15 kDa) and the  $\alpha$  subunit (130 kDa).

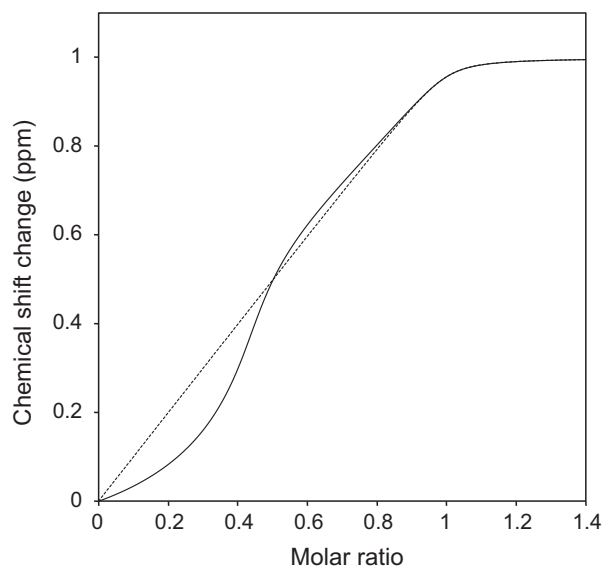
### 3.3. Chemical-shift titration

Chemical-shift titration is a simple method with which to map a ligand-binding site on a target protein and estimate  $K_D$ . Typically, an unlabeled ligand, such as a small compound, protein or nucleic acid, is titrated into an isotope ( $^{15}\text{N}$  and/or  $^{13}\text{C}$ )-labeled protein, and a 1D or 2D NMR spectrum of the protein is recorded after each ligand addition [21]. This very simple experiment has been applied to a large number of ligand–protein interactions. In the case of fast exchange, NMR signals appear at the population-averaged chemical shifts of the free and bound states, and  $K_D$  is estimated from curve fitting of the chemical shift changes as a function of the total concentrations of the protein ( $[A]_0$ ) and the ligand ( $[B]_0$ ) [42]:

$$\Delta\delta_{\text{obs}} = \frac{\Delta\delta_{\text{max}}}{2[A]_0} \left\{ K_D + [A]_0 + [B]_0 - \sqrt{(K_D + [A]_0 + [B]_0)^2 - 4[A]_0[B]_0} \right\} \quad (17)$$

where  $\Delta\delta_{\text{max}}$  is the chemical shift difference between the free and bound states in the case of slow exchange. In addition to  $K_D$ ,  $\Delta\delta_{\text{max}}$  is also estimated from the curve fitting. Eq. (17) is valid only when  $k_{\text{off}}$  is much larger than  $\Delta\omega$  ( $=2\pi\Delta\delta_{\text{max}}B_0$ ) because the exchange regime is always in fast exchange during the titration. It is important to treat both  $[A]_0$  and  $[B]_0$  as independent variables in the curve fitting to increase in the accuracy of the fitted  $K_D$  and  $\Delta\delta_{\text{max}}$  values [55]. Alternatively, the application of line shape analysis to a series of NMR spectra from a titration experiment provides accurate and precise kinetic parameters of the interaction such as  $k_{\text{off}}$  [56].

For some protein–ligand interactions, the observed resonances do not move linearly during a titration but instead follow curved tracks, which might indicate the presence of at least two binding modes. Even in such cases, the titration experiment in combination with singular value analysis can provide two distinct  $K_D$  values [57,58]. However, care must be taken in analyzing the curvature of chemical-shift changes because sigmoidal-like curvature can be observed even for the simplest single-binding interaction represented in Eq. (1) (Fig. 3). The singular value analysis is valid only for cases where the exchange regimes of all binding modes in the interaction are always in fast exchange during a titration. Because the exchange rate  $k_{\text{ex}}$  ( $= [B]k_{\text{on}} + k_{\text{off}}$ ) becomes faster with the increasing total ligand concentration  $[B]_0$  titrated into the protein solution, the exchange regime might vary during the titration. If the exchange regime of the interaction becomes intermediate or slow-to-intermediate at a certain value of  $[B]_0$ , an observable



**Fig. 3.** Example of chemical shift titration for a two-state exchange model. The solid and dotted lines were calculated by using the McConnell equation and Eq. (17), respectively. The calculations used  $\Delta\delta_{\max} = 1$  ppm,  $B_0 = 500$  MHz,  $k_{\text{on}} = 10^9$  M s<sup>-1</sup>,  $k_{\text{off}} = 2000$  s<sup>-1</sup>,  $K_D = 2$   $\mu$ M, and  $[A]_0 = 1$  mM. Under these conditions,  $\Delta\omega$  is always 3141 rad s<sup>-1</sup> during the titration, but  $k_{\text{ex}}$  increases with  $[B]_0$  (Eqs. (2) and (3)). For example,  $k_{\text{ex}}$  is 2105 s<sup>-1</sup> when  $[B]_0$  is 0.05 mM ( $k_{\text{ex}} < \Delta\omega$ ) and  $k_{\text{ex}}$  is 45733 s<sup>-1</sup> when  $[B]_0$  is 1 mM ( $k_{\text{ex}} > \Delta\omega$ ).

NMR signal of each spin will not appear at the population-averaged chemical shifts of the free and bound states or even at the chemical shift of the free or bound states. This change in the exchange regime during a titration causes sigmoidal curvature of the chemical shift changes, and the titration data must be analyzed by the Bloch-McConnell equation [59,60].

Kovrigin [61] computationally explored the chemical-shift titration patterns of various interaction systems including three-state exchange models using the Bloch-McConnell equation [59,61]. Interestingly, for some three-state exchange systems that comprise a mixture of fast and slow transitions, one NMR signal (e.g., bound resonance) exhibits a gradual shift of its position similar to fast exchange and the other NMR signal (free resonance) becomes weaker without changing its position as the ligand concentration increases similar to slow exchange. Mittag et al. [62] showed experimentally by using line shape analysis of the titration data that the interaction between the N-terminal src homology 2 domain of phosphatidylinositol-3-kinase and ligand peptide includes an intermediate state and the exchange system comprises a mixture of fast and slow exchange.

#### 4. Protein–ligand interactions in the intermediate- or slow-exchange regimes

When a protein–ligand interaction is in the intermediate- or slow-exchange regime, NMR quantities are not observed as population averages of the values in the free and bound states. NMR methods that are conducted under the assumption of population averaging due to fast exchange, such as chemical shift titration, transferred  $R_1$ , and transferred  $R_2$  experiments, cannot be applied to an intermediate- or slow-exchange interaction. In the chemical-shift titration experiment, for example, NMR signals of a protein or ligand do not move during a titration for a system in slow exchange, or for systems in intermediate exchange they may disappear at certain protein–ligand concentration ratios. Thus, a titration curve suitable for deriving the dissociation constant can-

not be drawn for either case. However, Latham et al. [28] determined the  $K_D$  value of the slow-exchange interaction between an RNA aptamer and the bronchodilator drug theophylline from a titration experiment. They measured the signal intensities of the free and the RNA–ligand complex resonances and estimated the bound fraction  $f_B$ , which varies according to the total concentrations of the RNA and drug in the NMR samples. Subsequently, the  $K_D$  value was calculated by replacing  $\Delta\delta_{\text{obs}}$  in Eq. (17) with  $f_B$ , and fitting the data to this modified equation. This simple method, however, is applicable only to cases where the transverse relaxation rate  $R_2$  of the bound state is either comparable to that of the free state or known a priori; otherwise, the fraction of the bound state might be underestimated because bound resonances relax faster than free resonances.

On the other hand, NMR methods that are designed to determine kinetic rates of intermediate- and slow-exchange systems, including protein–ligand interactions, have been developed, including  $R_2$  dispersion [24–26,63,64],  $R_{1\rho}$  dispersion [65,66], ZZ-exchange [27,67,68], chemical exchange saturation transfer (CEST) [69,70], and DEST [71]. These methods can be used to derive kinetic rates even though one of the states is not directly observable by NMR because of its low population and an excess relaxation rate,  $R_{\text{ex}}$ . For protein–ligand interactions,  $[B]k_{\text{on}}$  and  $k_{\text{off}}$  can be determined in the same way used to determine the kinetic rates of conformational exchange in a single molecule. Extracting  $k_{\text{on}}$  from  $[B]k_{\text{on}}$  is difficult, however, because  $[B]$  is also an unknown parameter that must be determined. In a typical sample for an interaction study using the above-listed NMR methods, the total concentration of B barely exceeds that of A, or does not exceed it at all. Therefore, only a very small fraction of B exists in the free state, making  $[B]$  difficult to determine experimentally. Demers and Mittermaier [72] determined  $K_D$  using ITC, and then calculated  $k_{\text{on}}$  according to  $K_D = k_{\text{off}}/k_{\text{on}}$  using  $k_{\text{off}}$  determined by NMR. As an alternative, methods based on  $R_2$  dispersion or ZZ-exchange spectroscopy have been developed to determine  $k_{\text{on}}$  and  $k_{\text{off}}$  with no previous information on  $K_D$ . In the following sections, we describe the theoretical and practical aspects of these  $R_2$  dispersion and ZZ-exchange methods.

##### 4.1. $R_2$ relaxation dispersion

$R_2$  relaxation dispersion spectroscopy is a transverse relaxation  $R_2$  experiment that can quantitate site-specific kinetic rates on the millisecond timescale, the population of each interconverting state, and chemical-shift differences between the states. A unique property of  $R_2$  dispersion is that it can probe low-populated minor states that are invisible to most biophysical methods.  $R_2$  dispersion has been used for dynamics studies of a multitude of proteins, such as enzymes [73–79], intrinsically disordered proteins [29–31,80], antibodies [81,82], human leukocyte antigen [83], and transcriptional activators [84]. Recently,  $R_2$  dispersion was even used to characterize the interaction between a <sup>15</sup>N-labeled small compound and an RNA aptamer [85].

Using  $R_2$  dispersion, a method was developed to determine  $k_{\text{on}}$  and  $k_{\text{off}}$  rates with no previous information on  $K_D$  [31]. Under the condition that the exchange of an association–dissociation process in equilibrium takes place on the millisecond timescale accompanied by relatively large chemical-shift changes, the effective relaxation rate  $R_2^{\text{eff}}$  of both the free and bound resonances increases by an excess relaxation rate,  $R_{\text{ex}}$ . Analysis of  $R_2^{\text{eff}}$  by the  $R_2$  dispersion experiment provides the exchange rate of the association–dissociation process  $k_{\text{ex}}$ , together with other parameters such as the chemical shift difference  $\Delta\omega$  between the free and bound states. For the two-state exchange model (Eq. (1)),  $R_2^{\text{eff}}$  is calculated via the equation derived by Carver and Richards [86]:

$$\begin{aligned}
R_2^{\text{eff}} &= R_{20} + \frac{1}{2} \left\{ k_{\text{ex}} - \frac{1}{\tau_{\text{CP}}} \cosh^{-1} [D_+ \cosh(\eta_+) - D_- \cosh(\eta_-)] \right\} \\
D_{\pm} &= \frac{1}{2} \left[ \pm 1 + \frac{\Psi + 2\Delta\omega^2}{\sqrt{\Psi^2 + \zeta^2}} \right] \\
\eta_{\pm} &= \tau_{\text{CP}} \sqrt{\frac{1}{2} \left( \pm \Psi + \sqrt{\Psi^2 + \zeta^2} \right)} \\
\Psi &= k_{\text{ex}}^2 - \Delta\omega^2 \\
\zeta &= 2\Delta\omega([B]k_{\text{on}} - k_{\text{off}}) \\
k_{\text{ex}} &= [B]k_{\text{on}} + k_{\text{off}}
\end{aligned} \quad (18)$$

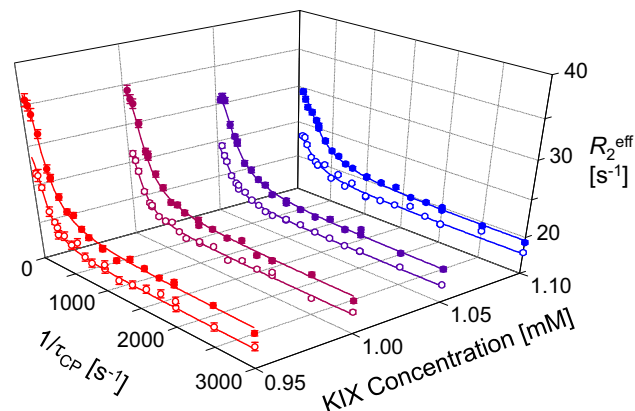
where  $R_{20}$  denotes the intrinsic relaxation rate, which is usually assumed to be identical for the free and bound resonances.  $\tau_{\text{CP}}$  denotes the delay between two successive  $180^\circ$  pulses in the Carr-Purcell-Meiboom-Gill pulse train.  $R_2^{\text{eff}}$  can also be calculated numerically via the Bloch-McConnell equation [59,87]. Provided that the protein–ligand interaction of interest is in the intermediate- or slow-exchange regime,  $k_{\text{ex}}$  can be separated into  $[B]k_{\text{on}}$  and  $k_{\text{off}}$ ; in the fast-exchange regime, however, only  $k_{\text{ex}}$ ,  $p_{\text{A}}p_{\text{B}}\Delta\omega^2$ , and  $R_{20}$  can be determined by  $R_2$  dispersion curve fitting.

As mentioned above, it is difficult to separate  $[B]$  and  $k_{\text{on}}$  from  $[B]k_{\text{on}}$ . Because Eq. (18) together with Eq. (2) indicates that  $k_{\text{ex}}$  depends on  $[A]_0$  and  $[B]_0$ ,  $k_{\text{on}}$  can be derived from a global fit of  $R_2$  dispersion profiles measured for multiple samples with different  $[A]_0$  and  $[B]_0$ . In practice,  $[A]_0$  (an isotope-labeled protein) is kept constant for a series of samples in order to measure  $R_2$  dispersion spectra at similar sensitivity, and  $[B]_0$  (an unlabeled target molecule) is varied. Thus, Eq. (2) is modified for the fitting of  $R_2$  dispersion profiles measured at multiple concentration ratios:

$$[B] = \frac{1}{2} \left\{ -K_D - [A]_0 + a[B]_0 + \sqrt{(K_D + [A]_0 - a[B]_0)^2 + 4a[B]_0 K_D} \right\} \quad (19)$$

where  $a$  denotes a ratio against a representative  $[B]_0$  value when  $a = 1$ , and is treated as a constant input parameter of the fitting for each NMR sample. Note that the experimentally determined concentrations  $[A]_0$  and  $[B]_0$  may contain some degree of error due to the experimental manipulations, which may in turn result in miscalculation of  $[B]$  and, of course, the fitting parameters such as  $k_{\text{on}}$  and  $k_{\text{off}}$ . For example, when  $K_D = 1 \mu\text{M}$ ,  $[A]_0 = 1 \text{ mM}$ , and  $[B]_0 = 1 \text{ mM}$ ,  $[B]$  is calculated to be  $31.1 \mu\text{M}$ . If  $[B]_0$  is wrongly determined to be  $0.95 \text{ mM}$ , corresponding to a 5% underestimation,  $[B]$  becomes  $14.5 \mu\text{M}$ , which is 0.466 times smaller than the correct value. To accurately determine the parameters by curve fitting, therefore, it is necessary to include the concentrations  $[A]_0$  and  $[B]_0$  in the variable fitting parameters. It should also be noted that NMR samples for the  $R_2$  dispersion experiments should be prepared carefully from a single concentrated stock solution of each molecule that has been dialyzed against the same buffer to render the concentration ratios accurate.

This  $R_2$  dispersion method was first applied to an intrinsically disordered protein—the phosphorylated kinase-inducible domain (pKID) of the transcription factor CREB, which binds to the KIX domain of CREB-binding protein (CBP) [31]. In that study,  $R_2$  dispersions of  $[^{15}\text{N}]$ -pKID were measured for samples with the KIX/pKID concentration ratios of 0.95, 1.00, 1.05, and 1.10 at the magnetic fields of 11.7 and 18.8 T. The measured  $R_2$  dispersions were concentration-dependent and the amplitude of  $R_{\text{ex}}$  decreased with the concentration of KIX (Fig. 4) because the population of the minor state (encounter complex) decreased with the concentration of KIX. The  $R_2$  dispersion curves at all four concentration ratios and at the two magnetic fields were fitted globally to the induced fit model (Eq. (6)), in which the chemical-shift differences  $\Delta\omega$  were treated as global parameters for each residue and the folding and unfolding rates  $k_1$  and  $k_{-1}$  were treated as global parameters for all residues in the cluster (neighboring residues within a local ele-



**Fig. 4.**  $R_2$  dispersion profiles for Arg124 in pKID.  $R_2$  dispersion data were recorded at 800 MHz (filled circles) and 500 MHz (open circles) for 1 mM  $^{15}\text{N}$ -pKID in the presence of 0.95, 1.00, 1.05 and 1.10 mM KIX. Reproduced with permission from [31]. The global fit of the  $R_2$  dispersion profiles provided  $k_{\text{on}}$ ,  $k_{\text{off}}$ ,  $k_1$ ,  $k_{-1}$ ,  $K_D$  in Eq. (6), and chemical shift differences between the encounter complex and bound state and between the encounter complex and intermediate state.

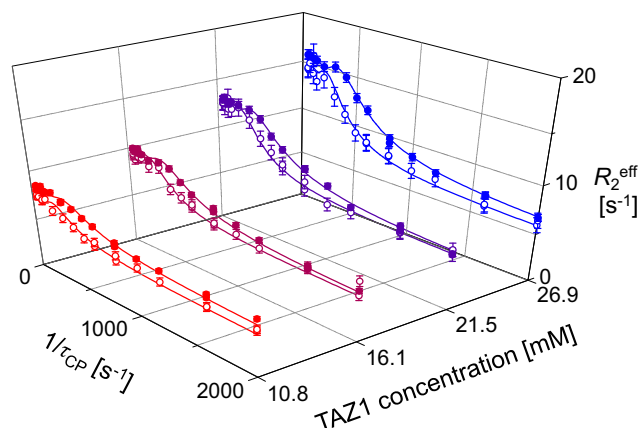
ment of secondary structure). This analysis provided site-specific  $K_D$  values for pKID, and the mean  $K_D$  value was in excellent agreement with the macroscopic  $K_D$  determined by ITC [88]. Together with chemical-shift titration experiments, the  $R_2$  dispersion experiments revealed that pKID forms encounter complexes via non-specific interactions while it is unfolded, and evolves via a partially folded binding intermediate to the fully folded bound state. Thus, the pKID–KIX interaction can be explained by a linear four-state exchange model, comprising the free, encounter complex, folding intermediate and bound states. In the analysis, however, this interaction was treated as a pseudo four-state exchange (a three-state exchange equivalent to the induced fit) under the assumption that the exchange between the free state and the encounter complex is too fast to be detected by  $R_2$  dispersion.

Recently, the same  $R_2$  dispersion method was applied to the transactivation domain of the transcription factor c-Myb, which is another KIX-binding intrinsically disordered protein [29]. The findings revealed that the N-terminal region of c-Myb binds to KIX in a predominantly folded conformation, whereas the C-terminal region folds via an induced-fit process after binding to KIX.

The same authors further developed the  $R_2$  dispersion method in order to determine  $k_{\text{on}}$ ,  $k_{\text{off}}$ , and  $K_D$  without observable bound resonances in systems where the population of the bound state is very low [30]. As mentioned above, association–dissociation processes that occur on the millisecond timescale with relatively large chemical shift changes influence the  $R_2$  relaxation rates of not only the bound but also the free resonances. Therefore,  $k_{\text{on}}$  and  $k_{\text{off}}$  can also be derived by analyzing  $R_2$  dispersion curves of free resonances measured for multiple samples containing an isotope-labeled protein and sub-stoichiometric amounts of the target molecule at different concentration ratios. For such samples, bound resonances are unobservable because of the low population and line broadening caused by chemical exchange. The bound state is therefore probed as a minor state by the analysis of  $R_2$  dispersion profiles.

This method was used to derive the  $k_{\text{on}}$ ,  $k_{\text{off}}$ , and  $K_D$  values of the interaction between an intrinsically disordered protein, Asn803-hydroxylated hypoxia-inducible factor-1 (HIF-OH), and the transcriptional adapter zinc-binding (TAZ1) domain of CBP [30]. The HIF-OH concentration was kept at  $510 \mu\text{M}$ , whereas the TAZ1 concentration was varied at 26.9, 21.5, 16.1, or  $10.8 \mu\text{M}$ . The  $R_2$  dispersion profiles obtained were concentration-dependent, and the amplitude of  $R_{\text{ex}}$  was found to increase with the concentration of





**Fig. 5.**  $R_2$  dispersion profiles for Glu817 in HIF-OH.  $R_2$  dispersion data were recorded at 900 MHz (filled circles) and 600 MHz (open circles) for 510  $\mu\text{M}$   $^{15}\text{N}$ -HIF-OH in the presence of 10.8, 16.1, 21.5 and 26.9  $\mu\text{M}$  TAZ1. Reproduced with permission from [30]. The global fit of the  $R_2$  dispersion profiles provided  $k_{\text{on}}$ ,  $k_{\text{off}}$ ,  $K_D$  in Eq. (1), and chemical shift difference between the free and bound states.

TAZ1 (Fig. 5) because the population of the minor state (the bound state in this case) increased with the concentration of TAZ1. Again, the derived  $K_D$  value was in excellent agreement with the macroscopic  $K_D$  determined by ITC. The chemical shift differences between the free and bound states  $\Delta\omega$  also agreed well with those calculated from the directly measured chemical shifts of the free and bound states.

For the bound state of TAZ1, the  $R_2$  dispersion profiles were almost flat lines ( $R_{\text{ex}} \approx 0 \text{ s}^{-1}$ ) because the exchange rate  $k_{\text{ex}} (= [\text{TAZ1}]k_{\text{on}} + k_{\text{off}})$  was too fast owing to its very large  $k_{\text{on}}$  ( $1.29 \times 10^9 \text{ M}^{-1} \text{ s}^{-1}$ ) and the high concentration of [TAZ1], as compared with the chemical shift difference between the free and bound states. The association rate,  $[\text{TAZ1}]k_{\text{on}}$ , is the only parameter that directly depends on the concentration ratio; thus, it is the key factor that determines the amplitude of  $R_{\text{ex}}$ . In other words, it is important to optimize the concentration ratio to obtain good  $R_2$  dispersion curves with a sufficient amplitude of  $R_{\text{ex}}$ . When  $k_{\text{on}}$  is very fast,  $R_2$  dispersions should be measured for the free state of a protein in the presence of sub-stoichiometric amounts of the target molecule. Furthermore, in the relatively common case that bound resonances are unobservable owing to intermediate exchange, relaxation dispersion measurements for free ligand resonances might provide chemical shifts of the bound state and hence valuable structural information on the complex.

To the best of our knowledge, this  $R_2$  dispersion method has not been applied to more complicated binding models. It is possible to calculate the concentration of free ligand numerically in more complicated models; however, it is not straightforward to determine accurate kinetic rate constants and chemical-shift differences by  $R_2$  dispersion curve fitting because there are numerous adjustable parameters, implying that a variety of parameter sets have a comparable quality of fit. A multitude of  $R_2$  dispersion data collected under different conditions, including concentration ratios, temperatures, magnetic field, and spin coherence, may be required to obtain the correct parameter set. For complicated exchange systems, it is more practical to analyze  $R_2$  dispersion data in combination with other NMR methods and/or biochemical manipulation of the protein. Indeed, four- and five-exchange systems have been characterized by such strategies (see Refs. [89–91]).

In contrast to this approach, Hansen et al. [38] developed a unique method based on  $R_2$  dispersion, which enabled the determination of  $k_{\text{on}}$ ,  $k_{\text{off}}$ , and  $K_D$  of the interaction between histone chaperone Chz1 and variant histone H2A.Z-H2B. They used a single NMR sample with a concentration ratio very close to 1:1. The affinity of the complex was relatively high ( $K_D \approx 0.2 \mu\text{M}$ ), and thus

both proteins were largely in the bound state with a small fraction in the free state. The unique strategy to derive  $k_{\text{on}}$  from a single sample was to uniformly label both Chz1 and H2A.Z-H2B with  $^2\text{H}$ ,  $^{15}\text{N}$ . The relaxation dispersions of both proteins were simultaneously measured, and the minor populations and the exchange rates of both proteins were independently estimated ( $[p_A, k_{\text{ex},A}]$  and  $[p_B, k_{\text{ex},B}]$ ) by curve fitting each set of relaxation dispersions. The  $K_D$  and  $k_{\text{off}}$  values were calculated by the following equations:

$$K_D = \frac{[A][B]}{[A:B]} = \frac{p_A p_B [A:B]}{(1-p_A)(1-p_B)} \approx p_A p_B [A]_0 \quad (20)$$

$$k_{\text{off}} = (k_{\text{ex},A} + k_{\text{ex},B}) \frac{p_A p_B}{p_A + p_B} \quad (21)$$

where A and B (including the subscripts) correspond to Chz1 and H2A.Z-H2B, respectively. Ultimately,  $k_{\text{on}}$  was calculated as  $k_{\text{on}} = k_{\text{off}}/K_D$ .

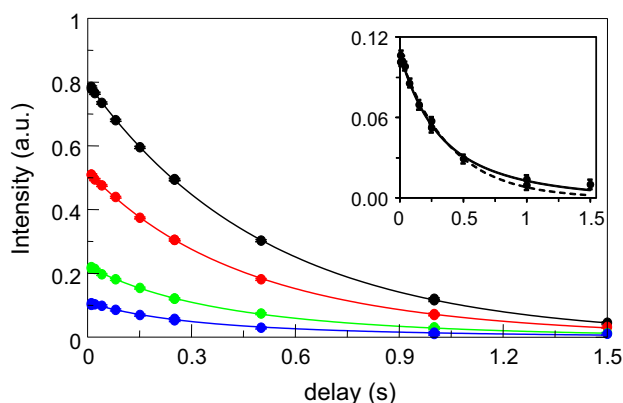
#### 4.2. ZZ-exchange

ZZ-exchange spectroscopy is a longitudinal relaxation technique to determine the auto-relaxation rates of two interconverting states that exchange on the millisecond to sub-second timescale [27]. This NMR method has been used to analyze the internal motions of proteins and binding kinetics of both protein–protein and protein–DNA interactions in the slow-exchange regime [32,67,68,92,93]. To quantitate binding kinetics by ZZ-exchange, the longitudinal relaxation profiles of the free and bound states and the two exchange peaks (i.e., free  $\rightarrow$  bound and bound  $\rightarrow$  free) of an isotope-labeled protein are analyzed simultaneously. It is essential to observe the free and bound resonances at the same time with signal intensities that are sufficiently high to allow the quantitation of auto-relaxation rates and exchange rates. For example, the sample would need to contain a half-stoichiometric amount of the target molecule.

Compared with  $R_2$  dispersion spectroscopy, ZZ-exchange spectroscopy has two unique properties that are important for characterizing binding kinetics. First, ZZ-exchange is more sensitive to slower molecular motions as compared with  $R_2$  dispersion. Because the longitudinal relaxation rates of proteins are usually slower than the transverse relaxation rates, slow molecular motions can perturb longitudinal magnetizations for longer during experimental relaxation delays. Second, ZZ-exchange does not require large chemical shift changes induced by binding to the target molecule because the longitudinal relaxation process is not affected by chemical shifts. In practice, free and bound resonances should be isolated sufficiently without peak overlap to quantitate their signal intensities. In contrast,  $R_2$  dispersion requires large chemical shift changes upon binding to the target molecule. In this regard, application of  $R_2$  dispersion is limited to flexible peptides or flexible regions of proteins, such as intrinsically disordered proteins, whereas ZZ-exchange can be used to quantitate the slow binding kinetics of a rigid protein whose chemical shifts (conformations) typically change little upon binding to the target molecule.

On the basis of these two properties of ZZ-exchange spectroscopy, Sugase developed a method to elucidate the slow binding events of a rigid protein, especially in cases where bound resonances are unobservable [37]. The concept of this approach is similar to that of the  $R_2$  dispersion method applied to HIF-OH/TAZ1, as described above. In the following explanation, we assume that there is no internal slow conformational rearrangement affecting the ZZ-exchange profile. ZZ-exchange spectroscopy is usually not applicable to cases where bound resonances are unobservable but, similar to  $R_2$  dispersion profiles, ZZ-exchange profiles of free resonances are modified by the association–dissociation process in a concentration-dependent manner as shown by Eq. (22) [27] for a two-state exchange model (Eq. (1)):





**Fig. 6.** ZZ-exchange profiles for Thr11 in GB1. ZZ-exchange data were recorded at GB1:IgG concentration ratios of 1:0 (black), 1:0.1 (red), 1:0.2 (green), and 1:0.3 (blue). The global fit of the ZZ-exchange profiles provided  $k_{\text{on}}$ ,  $k_{\text{off}}$ ,  $K_D$  in Eq. (1). The inset is a close-up view of the profiles for the 1:0.3 sample fitted with Eq. (22) (solid line) and Eq. (23) (dashed line). Reproduced with permission from [37].

$$I_F(t) = \frac{I_F(0)}{\lambda_+ - \lambda_-} [(\lambda_+ - R_{1F} - [B]k_{\text{on}}) \exp(-\lambda_- t) - (\lambda_- - R_{1F} - [B]k_{\text{on}}) \exp(-\lambda_+ t)]$$

$$\lambda_{\pm} = \frac{1}{2} \left[ R_{1F} + R_{1B} + [B]k_{\text{on}} + k_{\text{off}} \pm \sqrt{(R_{1F} - R_{1B} + [B]k_{\text{on}} - k_{\text{off}})^2 + 4[B]k_{\text{on}}k_{\text{off}}} \right] \quad (22)$$

where  $R_{1F}$  and  $R_{1B}$  denote the auto-relaxation rates of the ligand in the free and bound states, respectively. Similar to the  $R_2$  dispersion method,  $[B]$  is calculated by Eq. (19), and it is also necessary to include the concentrations  $[A]_0$  and  $[B]_0$  in the fitting parameters. When  $[B]_0$  is zero, corresponding to the situation that A is completely in the free state, Eq. (22) can be simplified as:

$$I_F(t) = I_F(0) \exp(-R_{1F}t) \quad (23)$$

The curve drawn by this equation is identical to the longitudinal relaxation profile measured in the regular  $R_1$  relaxation experiment. Therefore, the auto-relaxation rate of the free state  $R_{1F}$  in Eq. (22) can be independently determined.

The ZZ-exchange method is similar to the transferred  $R_1$  experiment described above; however, the application of the transferred  $R_1$  experiment is limited to the condition of fast exchange. A major difference between this ZZ-exchange method and the transferred  $R_1$  method is their mathematical treatments for determining the dissociation constant from relaxation profiles. In ZZ-exchange, the dissociation constant is calculated from the binding kinetics  $k_{\text{on}}$  and  $k_{\text{off}}$  ( $K_D = k_{\text{off}}/k_{\text{on}}$ ). In transferred  $R_1$ , by contrast, the  $R_1$  relaxation rate is measured as a population-averaged value of the free and bound states of a ligand (Eq. (15)). The difference between  $R_{1F}$  and  $R_{1B}$  should be large enough to quantitate  $p_B$  accurately for the transferred  $R_1$  method using Eq. (15). From another viewpoint, Eq. (16) indicates that the transferred  $R_1$  method cannot determine  $k_{\text{on}}$  and  $k_{\text{off}}$  rates. In contrast, the ZZ-exchange method is applicable even in the case where the difference  $R_{1F}$  and  $R_{1B}$  is small if  $[B]k_{\text{on}}$  and  $k_{\text{off}}$  perturb the ZZ-exchange profile, which is defined by  $[B]k_{\text{on}}$  and  $k_{\text{off}}$ , as well as  $R_{1F}$  and  $R_{1B}$  (Eq. (22)).

Sugase applied the ZZ-exchange method to interaction between the B1 domain of *Streptococcus* protein G (GB1), a rigid globular protein composed of 56 residues, and immunoglobulin G (IgG) [37]. Previous structural studies indicated that GB1 binds to each of the two heavy chains in the Fc region of IgG with little conformational change [94,95]. The binding kinetics of this interaction could not be analyzed by the  $R_2$  dispersion method described above. In the ZZ-exchange experiment, the GB1 concentration was kept at 200  $\mu\text{M}$ , whereas the IgG concentration was varied at 0, 20, 40, or 60  $\mu\text{M}$ . The ZZ-exchange profiles obtained were concentration-dependent (Fig. 6). The inset shows that later points deviate more from the theoretical curve calculated with Eq. (23)

(the regular  $R_1$  experiment) than from that calculated with Eq. (22) (the ZZ-exchange experiment). The ZZ-exchange experiments enabled us to determine  $k_{\text{on}}$  ( $1.50 \times 10^7 \text{ M}^{-1} \text{ s}^{-1}$ ),  $k_{\text{off}}$  ( $2.23 \text{ s}^{-1}$ ), and consequently,  $K_D$  (149 nM).

## 5. Conclusion

We described that NMR is a very powerful tool to analyze protein–ligand interactions quantitatively. There are various NMR methods, and it is essential to choose one that is appropriate for analyzing the protein–ligand interaction of interest. In particular, the exchange regime of the interaction is one of the most important factors in selecting an appropriate method. Even for a simple chemical shift titration experiment, the simplest equation (Eq. (17)) for determining  $K_D$  from the chemical shift data is not always valid.

The recent advent of new relaxation experiments has enabled us to characterize slower protein–ligand interactions in detail. Such relaxation experiments provide kinetic information on interactions but, again, it is critical to choose an appropriate kinetic model, such as a two- or three-state exchange model, to derive correct kinetic information. How can we validate whether the chosen model is appropriate? There is no general rule, but it must be confirmed, at least, that the parameters obtained are physiologically reasonable and consistent with previous data, and the fitting quality of a certain model is statistically better than that of other models. For example, if the  $k_{\text{on}}$  obtained is more than  $10^{10} \text{ M}^{-1} \text{ s}^{-1}$ , the chosen model might be inappropriate, whereas if the  $K_D$  obtained is comparable to that determined by another method, the chosen model is likely to be appropriate. In terms of comparing the fitting quality, the  $F$ -test and Akaike's information criterion are often used [96].

We have also described two recent types of NMR method that utilize  $R_2$  dispersion or ZZ-exchange. Both methods can determine the binding kinetics and dissociation constant. Essential steps in both methods are the careful preparation of multiple NMR samples with different concentration ratios and global data analysis using an appropriate kinetic model [39]. Because the pulse programs were not modified, it would be easy to extend these methods to larger protein–ligand interactions by adopting TROSY-type measurements [63,64,67,68]. It should also be possible to develop similar methods using other NMR measurements such as CEST [69,70], DEST [71], or  $R_{1\rho}$  dispersion [65,66], or other spin types of  $R_2$  dispersion [97–102].

NMR has firmly established its position in studies of protein–ligand interactions. Furthermore, new NMR methods are still being developed to analyze difficult protein–ligand interactions and to obtain more detailed insight into them. As a result, NMR will remain central to such studies or even elevate its position in future research.

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## Glossary of abbreviations

CBP: CREB-binding protein  
 CEST: chemical exchange saturation transfer  
 DEST: dark-state exchange saturation transfer  
 GB1: the B1 domain of *Streptococcus* protein G  
 HIF-OH: hydroxylated hypoxia-inducible factor-1  
 IgG: immunoglobulin G  
 ITC: isothermal titration calorimetry  
 pKID: phosphorylated kinase-inducible domain  
 STD: saturation-transfer difference  
 TAZ1: transcriptional adapter zinc-binding  
 WaterLOGSY: water-ligand observed via gradient spectroscopy